

REVIEW

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Cockle shell-derived aragonite calcium carbonate nanoparticle for targeting cancer and breast cancer stem cells

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Abstract

Cockle shell-derived aragonite calcium carbonate nanoparticles (CACNP) have demonstrated prospect as nano-sized drug carriers for targeting cancer cells. CACNP is biocompatible, biodegradable and its biomaterial is readily available and is of low cost. In addition, CACNP is highly porous, has a large surface area which confer a high loading capacity. The pH-dependent release properties as well as its potential for surface functionalization with targeting agents make CACNP useful in passive and active targeting of cancer cells and cancer stem cells. In this article, we reviewed the current state of CACNP as nano-sized drug carrier for targeting cancer cells, cancer stem cells and its biocompatibility.

Keywords: Calcium carbonate nanoparticle, Cockle shell, Biocompatibility, Cancer therapy

Introduction

Cancer arises from multiple mutations in the genome which results in interruption in the normal cellular homeostasis. This disruption in cellular homeostasis drives normal cells to acquire a succession of hallmark capabilities that allow them to become tumorigenic and eventually malignant. These hallmark capabilities include replicative immortality, genomic instability, evasion of growth suppression, resisting cell death, sustained proliferation, altered metabolism, avoiding immune destruction, use tumour promoting inflammation to their advantage, angiogenesis induction, activation of process of invasion and metastasis. Continuous uncontrolled replication results in colony of abnormal cells which are heterogeneous in nature; interacting with each other and the extracellular component (Hanahan and Weinberg 2000, 2011; Sancho et al. 2016). The efficacy of conventional chemotherapeutic agent is limited by systemic toxicity and multidrug resistance. Nonetheless significant progress has been made in the field of nanotechnology to overcome these problems, thus offering promising and effective alternatives for cancer treatment (Blanco et al. 2015). Nanotechnology has shown a great advantage in drug delivery for cancer treatment by enhancing build-ups of cytotoxicity in tumour tissue, specificity in tumour targeting, reducing the cytotoxic side effects on normal cells,



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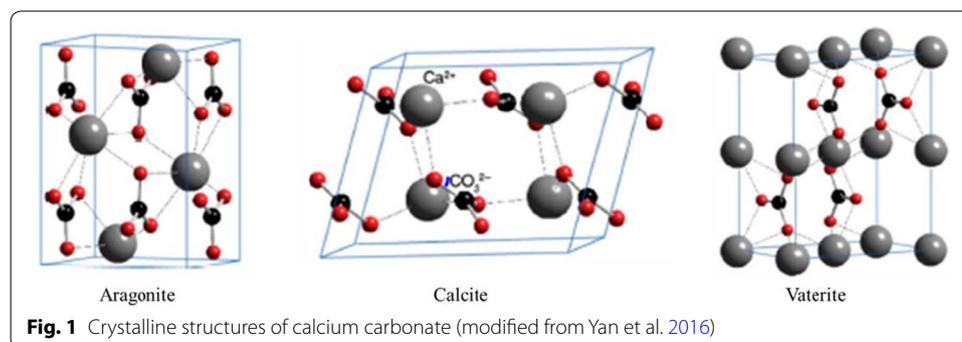
reducing systemic side effect, increasing drug solubility, and increasing maximum tolerated dose.

Cockle shell-derived aragonite calcium carbonate nanoparticles (CACNP) have demonstrated prospect as nano-sized drug carriers for targeting cancer cells. CACNP is biocompatible, biodegradable and its biomaterial is readily available and is of low cost. In addition, CACNP is highly porous, has a large surface area which confer a high loading capacity. The pH-dependent release properties as well as its potential for surface functionalization with targeting agents make CACNP useful in passive and active targeting of cancer cells and cancer stem cells. Hence, this article reviews the available literatures on CACNP as drug delivery system for targeting cancer cells (Mailafiya 2019a).

Calcium carbonate nanoparticles

CaCO_3 is an important industrial mineral that is used in most sphere of human life (Horie 2014; Lauth et al. 2017). The characteristic high surface area and small size favours its use in food, paint, rubber, cosmetic, cement and stationary industries (Horie 2014). Six crystal morphologies of CaCO_3 has been reported namely; calcite, vaterite, aragonite, amorphous calcium carbonate, ikaite and monohydrocalcite (Lauth et al. 2017). Anhydrous CaCO_3 has three polymorphs—calcite, vaterite and aragonite (Fig. 1), which have been tried for controlled drug delivery (Lauth et al. 2017). The calcite polymorph exists as trigonal crystalline form in nature while the aragonite and vaterite polymorphs are seen as orthorhombic and hexagonal systems, respectively (Dizaj et al. 2015). The polymorphs can be differentiated based on spatial arrangement of the calcium and carbonate ions which determines their stability and solubility (Mydin et al. 2018; Dizaj 2015). Calcite is the most thermodynamically stable and least soluble in water followed by aragonite (Boulos (2014); Kezuka et al. 2017). Vaterite on the other hand, is the least stable and most soluble in water (Boulos (2014)). The vaterite polymorph easily changes to either aragonite at 30 °C or calcite at 60–80 °C (Boulos 2014; Li et al. 2019). The three polymorphs can be found simultaneously in some types of molluscs and sea algae, but calcite and aragonite are more common (Ni and Ratner 2008).

Recently, the fabrication and therapeutic application of CaCO_3 nanoparticles in drug delivery has generated a lot of attention amongst scientists due to its availability, ease of synthesis, low toxicity and slow biodegradability (Mydin et al. 2018; Dizaj 2015; Li et al. 2019). CaCO_3 nanoparticles have been synthesized using various methods including wet chemical preparation, microemulsion technique and mechanical milling of sea and egg



shells (Mydin et al. 2018; Dizaj 2015; Ranjan et al. 2018). Ghiasi and Malekzadeh (2012) used the sol–gel citrate method to synthesize calcite nanoparticles by adding organic additives as emulsifiers. The main advantage of this citrate method is that it lowers the calcination temperature (Ghiasi and Malekzadeh 2012). CaCO_3 nanoparticles have also been synthesized by thermolysis of a precursor molecule, calcium oxalate—a low-cost method that can be used for bulk production of calcium carbonate nanoparticles (Ranjan et al. 2018). Monodispersed CaCO_3 nanoparticles was synthesized using batch carbonation process with ultrasonication (He et al. 2005). The advantage of this method is that it produced CaCO_3 nanoparticles of small and narrow size distribution (He et al. 2005). The use of natural reserves of calcium carbonate such as egg shells and cockle shell to synthesize CaCO_3 nanoparticles is advantageous because it is readily available, non-toxic, and biocompatible as well as manage wastes from processing these foods as such this makes ideal candidates for biomedical applications (Render 2016; Idris et al. 2019).

Cockle shell-derived aragonite calcium carbonate nanoparticle

One of the most important considerations for nanoparticle design is the safety of the delivery system. The materials for designing nanoparticle must be biodegradable, biocompatible and should not produce toxic by-products (Vishwakarma et al. 2010; Wolf-ram 2015). In addition, nanoparticle should have high drug-loading capacity with maximum drug release from the particle at the tumour site and the surface charge of the nanoparticle must be within the stability range > 25 mV and < -25 mV (Honary and Zahir 2013a, b). The size of the nanoparticle needs to be optimal for systemic administration. Too large particles result in embolus formation while particles less than 10 nm are rapidly cleared from the circulation. The nanoparticle size range of 50 nm to 100 nm showed enhanced passive targeting by the EPR effect (Xu et al. 2015). The production of the nano-sized particle should be simple and allows for scale-up.

Cockle shell-derived aragonite calcium carbonate nanoparticle (CACNP) has a promising potential and it is an ideal nanomaterial for drug delivery due to its higher surface area, surface structural porosity with large loading content capacity, pH-dependent drug release, biocompatible and biodegradable (Mailafiya 2019a). The preparation of CACNP involves top down mechanical milling and/ or the use of BS-12; a simple synthesis method to produce large-scale nanoparticles that is cost effective and utilize the natural abundance of cockle shell (Xu et al. 2015). CACNP has also been prepared by dissolution precipitation method (Tram 2020) and higher pressure homogenizer micro-emulsion technique (Kamba 2013). The structural surface porosity CACNP encourages the incorporation of both hydrophilic and hydrophobic drugs with increase drug loading and encapsulation efficiency (Mailafiya 2019a).

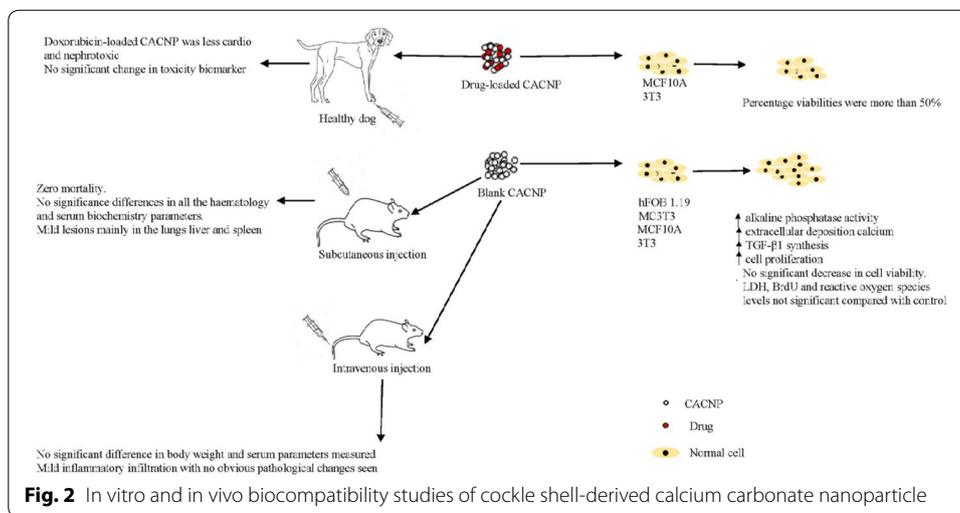
CACNP appears as rod-to-spherical when observed with transmission electron microscopy (TEM). Both pleomorphic and homogeneous surface morphology under field emission scanning electron microscopy (FESEM) has been described. The size ranges from 11 to 100 nm with overall negative surface charge. XRD and FTIR analysis of drug-loaded CACNP have shown that drugs loaded within the nanoparticles maintained their crystallinity and functionality, respectively, within the nanoparticle as well as demonstrating effective loading of the drug. The colloidal stability of

CACNP was investigated by Danmaigoro et al. (2017). They reported the stability of CACNP maintained in aqueous solvent at pH 7.9 for 5 months at 50 °C. The stability was attributed to stability of aragonite polymorph of calcium carbonate. The physicochemical properties of CACNP are summarized in Table 1.

Nonetheless, CACNP have exhibited promising potential as targeting nano-sized carriers against cancer cells. CACNP has also been used in osteoporosis therapy and hormonal delivery (Jaji 2017) as well as scaffolds for bone repair and tissue engineering (Bakar et al. 2011; Mahmood et al. 2017a, b). The pH-sensitive characteristic of CACNP provide a possibility of targeting cancer cells and controlled delivery of anti-cancer drugs. The sustainability of drug delivery as a result of the slow degradation of CaCO₃ nanoparticles combined with potential to specifically target cancer cells, which results from their prospect to be functionalized with targeting compounds, are key features. Surface functionalization of CaCO₃ nanoparticle opens a new perspective to actively target cancer cells or cancer stem cells. This combination leads to targeted and effective drug delivery for cancer diagnosis and treatment (Maleki Dizaj et al. 2015; Dizaj 2019; Abd Ghafar et al. 2017).

Table 1 Summary of physicochemical properties of cockle shell-derived calcium carbonate nanoparticles

Mode of CACNP preparation	XRD pattern	Encapsulation efficiency (%) / drug loaded	Size and shape viewed with TEM	Zeta potential	References
Cockle shell dissolved with hydrochloric acid + CaCl ₂ + Na ₂ CO ₃ + calcination	Calcite		50-100 nm,		Tram (2020)
Higher pressure homogenizer (HPH) microemulsion system	Aragonite	64–96% doxorubicin	12–30 nm rod-shaped, pleomorphic		Kamba (2013), Kamba et al. (2013a)
		99.5% ciprofloxacin	11.93 to 22.12 nm spherical shaped, pleomorphic		Isa et al. (2016)
Cockle shell microparticles with surfactant BS-12 stirred at 80 °C for 90 min	Aragonite	54% vancomycin	34 ± 5–36 ± 6 nm, cubic shaped, pleomorphic	− 19.4 ± 3.3 mV	Saidykhan et al. (2016)
Cockle shell microparticles with surfactant BS-12 stirred at 27 °C for 2 h	Aragonite	93.8% to 97% doxorubicin	29.7 ± 5 nm, spherical, pleomorphic	− 19.1 ± 3.9 mV	Hamidu (2019)
Mechanical method	Aragonite	58.9% cytarabine	Diameter ranging from 20 to 50 nm, oval, homogeneous,	− 11 mV	Ghaji (2018)
Cockle shell microparticles with surfactant BS-12 stirred at 27 °C for 2 h + mechanical method	Aragonite	95% to 99% doxorubicin	24.9 ± 4.07 nm, spherical, homogeneous	− 21 mV	Danmaigoro et al. (2017)
		32% to 99% curcumin	21.38 ± 2.7 nm spherical, pleomorphic	− 18.7 mV	Mailafiya (2019b)
Cockle shell microparticles with surfactant BS-12 stirred 50 °C for 135 min + mechanical method	Aragonite	Gold	35 ± 16 nm, spherical, pleomorphic	− 16.4 ± 3.81 mV	Kiranda et al. (2018)



CACNP as a drug delivery system

Drug loading is an important in achieving efficient nanomaterial drug delivery. Nanomaterial with high degree of loading capacity are principally required for drug administration. Due to the porosity of cockle shell-derived calcium carbonate nanoparticle, it is capable of loading different drugs irrespective of their hydrophobicity or surface charge. The application of CACNP as a drug delivery system is summarized in Table 1.

Cockle shell-derived calcium carbonate nanoparticles have successfully encapsulated cytarabine (Ghaji et al. 2018), docetaxel (Hammadi 2017a), doxorubicin (Danmaigoro et al. 2017; Kamba and Zakaria 2014; Fu 2017; Hamidu 2019), thymoquinone (Ibiyeye et al. 2020), parathyroid hormone (Jaji 2017), ketoprofen lysinate (Ghafar et al. 2017), ciprofloxacin (Isa et al. 2016), vancomycin (Saidykhan et al. 2016), oxytetracycline (Idris et al. 2019) and curcumin (Mailafiya 2019b). CACNP has been successfully loaded with both hydrophilic and hydrophobic drugs and their combination. CACNP has also been conjugated with gold as a nano-hybrid biomaterial for possible cancer imaging (Kiranda et al. 2018).

Biocompatibility of CACNP

Nano-sized materials are relatively unsafe. The characteristics of nano-sized materials are relatively different from larger particles of the same material. Safety of nano-sized materials have been shown to be dependent on nanoparticle morphology. Similarly, the size of nanoparticles is also important in determining biocompatibility. The decrease in particle size and larger surface area make them assimilate better in the body fluids and tissues thereby increasing their toxicity (Vishwakarma et al. 2010; Wolfram 2015). Gold nanoparticles of 1.4 nm size were found to be toxic, while 15 nm was not toxic at a concentration as high as 100-fold increase (Pan et al. 2007). CACNP size range may contribute to its safety. Unlike other nanoparticles, CACNP have shown no cytotoxic effect in normal cells and in in vivo studies (Fig. 2). CACNP has been shown to be safe on MCF10A, 3T3 mouse fibroblast cells, MC3T3 E-1 osteoblast cells, hFOB 1.19 human foetal osteoblastic cells (Kamba and Zakaria 2014; Fu 2017; Ibiyeye et al. 2020; Kiranda et al. 2018; Kamba et al. 2013a, 2014a; Hammadi 2017b).

Hammadi et al. (2017a) recorded the cell viability of MCF10A to be more than 90% at a concentration of 1000 $\mu\text{g/ml}$. Ibiyeye et al. (2019) also recorded cell viability of 80% when MCF10A and 3T3 were exposed to a concentration of 1000 $\mu\text{g/ml}$ of CACNP. About 60% cell viability was observed in 3T3 cells when exposed to gold–CACNP hybrid nanoparticle at 100 $\mu\text{g/ml}$ concentration. On the other hand, 25 $\mu\text{g/ml}$ of gold–CACNP increased 3T3 viability (Kiranda et al. 2018). Idris et al. observed the percentage cell viability of NIH3T3 cells to be 82.7% after 72 h treatment with 100 $\mu\text{g/ml}$ CACNP. Kamba et al. (2013a) researched the effect of CACNP (0 to 400 $\mu\text{g/ml}$) on NIH 3T3 cell line using various assays including MTT, LDH, BrdU and reactive oxygen species level. No significance differences was observed in all the parameters measured when compared with control. The percentages cell viability were 92% and 85% at concentrations of 200 and 400 $\mu\text{g/ml}$, respectively (Ibiyeye et al. 2019).

Kamba and Zakaria (2014) evaluated the response of 200 $\mu\text{g/ml}$ of CACNP on hFOB 1.19 and MC3T3 E1 osteoblast cells for 1 to 3 days. Increase in cell proliferation was noticed for both cells. The alkaline phosphatase activity of these cells increased significantly over time. Both cells produced significant amounts of intracellular protein when compared with the control. hFOB 1.19 and MC3T3 E-1 cells cultured with CACNP showed increase in extracellular deposition calcium when compared with control. A significant increase in TGF- β 1 synthesized by hFOB 1.19 and MC3T3 E-1 cells was observed when compared with control as well as increased production of VEGF in a time-dependent manner. Kamba and Zakaria concluded that CACNP encourage osteoblast differentiation and advance osteo-integration processes. Fu et al. (2017) noticed that when the hFOB 1.19 human foetal osteoblastic cells were exposed to high concentrations of CACNP at 500–1000 mg/ml , the cell viability percentages were greater than 70% (Fu 2017). CACNP and parathyroid hormone-loaded CACNP increased hFOB 1.19 cell proliferation best at 24 and 48-h time periods, whereas parathyroid hormone-loaded CACNP has the highest cell viability at the 72-h period (Jaji 2017). Jaji (2017) concluded that CACNP is a facilitator of osteoblast proliferation and an efficient nanocarrier for sustained release of parathyroid hormone (Jaji 2017). Ghafar et al. (2017) analysed the cytotoxicity of surface-functionalized CACNP and CACNP without surface modification on hFOB 1.19. The percentage cell viability of surface-functionalized CACNP (90.1%) was higher compared with CACNP without surface modification (79.5%) at a dose 1000 $\mu\text{g/ml}$. Surface modification of CACNP was observed to improve biocompatibility of CACNP (Ghafar et al. 2017).

Safety of CACNP have been demonstrated in vivo (Jaji et al. 2017; Chunyan et al. 2019). Jaji et al. (2017) evaluated the single and repeated subcutaneous dose of CACNP in SD rats. A single subcutaneous dose of 29,500 mg/m^2 was given and closely monitored for 14 days. Also, 28 days repeated doses of 59, 590 and 5900 mg/m^2 of CACNP were studied. Zero mortality was documented at the end of both studies. The 59 mg/m^2 -dose group showed no significance differences in all the haematology and serum biochemistry parameters measured when compared with the control while there were significance differences in almost all parameters for 5900 mg/m^2 dose group. The 59 mg/m^2 and 590 mg/m^2 -dose groups showed mild lesions mainly in the lungs liver and spleen. Single-dose 29,500 mg/m^2 and 5900 mg/m^2 -dose group showed severe lesions in major organs. Jaji et al. concluded that 59 mg/m^2 marked the safety margin of CACNP in SD

rats. Chunyan et al. (2019) administered intravenous dose of 0, 30 mg/kg, 60 mg/kg and 120 mg/kg CACNP to SD rats daily for 14 days. Two mortalities were recorded in 120 mg/kg group. There was no significant difference in body weight and serum parameters measured in all treatment groups compared with control. The histological changes observed in intravenous administration of 30 mg/kg CACNP include mild inflammatory infiltration with no obvious pathological changes seen while the 60 mg/kg and 120 mg/kg groups showed obvious histological changes in main organs.

The safety of drug-loaded CACNP has been evaluated in non-neoplastic cells and healthy dogs (Ibiyeye et al. 2019; Danmaigoro 2018; Idris 2020). Ibiyeye et al. (2019) observed the cell viability of doxorubicin-loaded CACNP, thymoquinone-loaded CACNP and combined doxorubicin–thymoquinone-loaded CACNP on 3T3 and MCF10A. The percentage viabilities were more than 50% at 24, 48 and 72 h after treatment for both cells. Danmaigoro (2018) evaluated the effects of repeated intravenous administration of doxorubicin-loaded CACNP on healthy dogs. Dogs were administered 5 cycles of doxorubicin-loaded CACNP 50 mg/m² (high dose), 30 mg/m² (clinical dose) and 20 mg/m² (low dose) every 3 weeks. 30 mg/m² and 20 mg/m² treatment doses did not show any significant change in toxicity biomarker when compared with the control. Doxorubicin-loaded CACNP was less cardio and nephrotoxic at 50 mg/m² dose when compared to dogs given equivalent free doxorubicin. The cytotoxicity of oxytetracycline-loaded CACNP and free oxytetracycline was evaluated in NIH3T3 cells for 72 h. The percentage cell viability of oxytetracycline-loaded CACNP (75.5%) was higher compared to free oxytetracycline (66.0%) at 100 µg/ml. Loading oxytetracycline into CACNP was observed to increase the biocompatibility of oxytetracycline (Idris 2020).

Application of drug-loaded CACNP on cancers

Nano-sized particles with diameters less than 600 nm as the advantage of enhanced permeation and retention effect at the site of cancerous tissues which facilitates the concentration of drugs in tumour environment. Moreover, calcium carbonate nanoparticles have unique liquid-phase characteristics which enable it to be stable at physiologic; in acidic pH they disintegrate. This property has been exploited to deliver drug-loaded CACNP to cancer environment and intracellular lysosome where they disintegrate releasing their constituents (Dizaj 2015). Electrostatic interactions between the negatively charged CACNP and the cancer cell membrane are of great biological importance. The adhesion of negatively charged nanoparticles to the cell membrane exerts a strong influence on the structure of the membranes by formation of a high-density domain of lipid tails, this facilitates their internalization into cancer cells via endocytosis (Behzadi 2017). These account for CACNP cytotoxicity. The cytotoxicity of drug-loaded CACNP (Table 2) has been demonstrated on different breast cancer cell lines (Hammadi 2017a, b; Kamba and Zakaria 2014; Kiranda et al. 2018; Kamba et al. 2013a, 2014b; Ibiyeye et al. 2019), osteoblastic and human osteogenic cell lines (Jaji 2017; Kamba and Zakaria 2014; Fu 2017; Kamba et al. 2013b), human leukemic cells (Ghaji 2018) and breast cancer enriched mammosphere (Ibiyeye and Zuki 2020). Drug-loaded CACNP was also demonstrated in breast cancer breast-bearing Balb/C mice (Hammadi 2018), murine xenograft leukemic model (Ghaji 2018), orthotopic osteosarcoma bearing rats (Fu 2018), and in evaluating the toxicity effects of repeated dose of doxorubicin loaded CACNP in

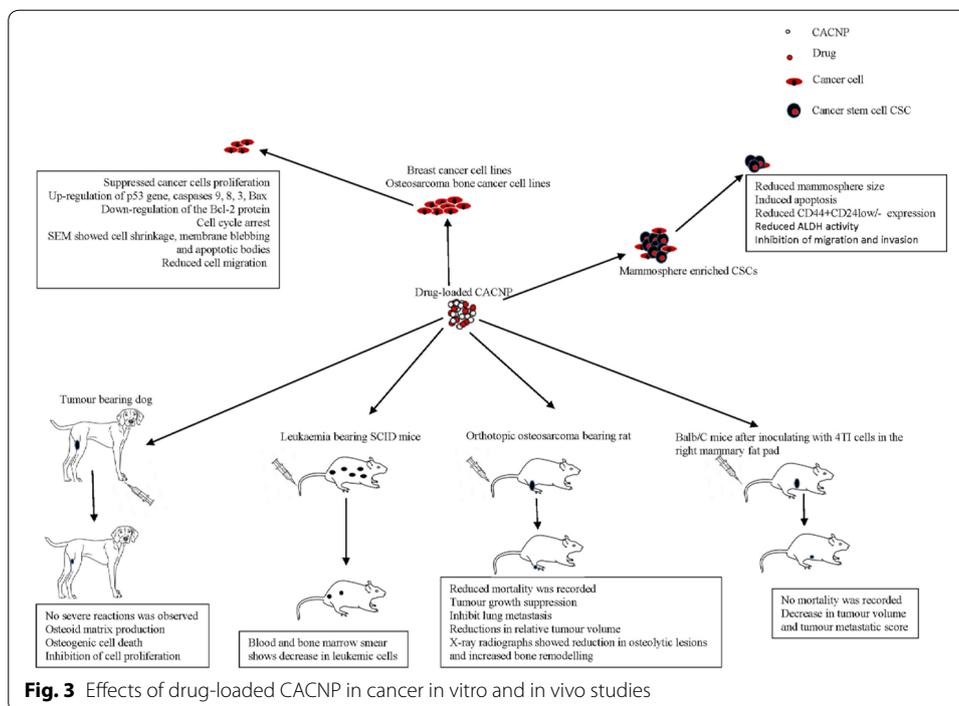
Table 2 Summary of drug-loaded CACNP and their outcomes in cancer cells

Drug loaded into CACNP	Response	References
Doxorubicin	Doxorubicin-loaded CACNP was effective in killing MCF-7 and MDB 231 compared to free doxorubicin in a time-dependent manner	Kamba et al. (2013a, 2014b)
	Sensitivity of MCF-7 cell to free doxorubicin and doxorubicin-loaded CACNP was time dependent	Hamidu (2019)
	Doxorubicin-loaded calcium carbonate nanoparticle caused death of MG 63 cell by induction of apoptosis. Induction of apoptosis was by up-regulation of p53, Bax and caspases 3, 8 and 9 and down-regulation of the Bcl-2 protein	Kamba et al. (2013b)
	Doxorubicin-loaded CACNP showed a similar reduction in cell viability as free doxorubicin in a concentration and time-dependent manner	Fu (2017)
	Doxorubicin-loaded CACNP significantly reduced osteosarcoma tumour volume and doxorubicin-related cardiotoxicity in osteosarcoma bearing rats	Fu (2018)
Doxorubicin, thymoquinone	Partial response and progressive canine RECIST response	Danmaigoro (2019)
	Doxorubicin–thymoquinone-loaded CACNP was the most efficient in eliminating breast cancer cells at a lower dose of doxorubicin and thymoquinone	Ibiyeye et al. (2019)
Gold	Doxorubicin–thymoquinone-loaded CACNP was most effective among the loaded CACNP in inhibiting CSCs' properties	Ibiyeye and Zuki (2020)
	Gold-conjugated calcium carbonate nanoparticle progressively decreased the percentage cell viability of MCF-7 cells	Kiranda et al. (2018)
Docetaxel	Free docetaxel and docetaxel-loaded CACNP revealed a progressive reduction in percentage viability of MCF-7 cancer cells in a dose and time-dependent manner	Hammadi (2017a)
	Docetaxel-loaded CACNP and free docetaxel has similar anticancer effects on 4T1 cells	Hammadi (2017b)
	Tumour volume, organ weight, tumour inhibition rate, and tumour metastatic score were significantly lowered in breast cancer bearing docetaxel-loaded CACNP 10 mg/kg Balb/C mice. group	Hammadi (2018)
Cytarabine	Cytarabine-loaded calcium carbonate nanoparticle significantly ameliorated the cancer effect in major organs of leukaemia-bearing SCID mice	Ghaji (2018)

healthy (Danmaigoro 2018) and tumour bearing dogs (Danmaigoro 2019). The effects of drug-loaded CACNP on various cancers (Fig. 3) are discussed below.

Application of drug-loaded CACNP on breast cancer

Kamba et al. (2013a, 2014b) evaluated the effect of free doxorubicin and doxorubicin-loaded CACNP on MCF-7 and MDB 231 breast cancer cell line. MTT, neural red, and lactate dehydrogenase colorimetric assays revealed higher toxicity of doxorubicin-loaded CACNP and effective cells killing compared to free doxorubicin in a time-dependent manner. Result of MCF-7 TUNEL assay verified that most of the cells undergoes apoptosis by internucleosomal fragmentation of genomic DNA (Kamba et al. 2014b). A significant increase in the amount of fragmented DNA was observed from 24 to 72 h. Time and dose-dependent increase in Bax, cytochrome C and caspase-3 protein expression were observed (Kamba et al. 2013a, 2014b). Cell clumping, apoptotic bodies and membrane blebbing were apparent in the scanning electron



microscope (SEM) analysis (Kamba et al. 2014b). Hamidu also evaluated free doxorubicin and doxorubicin-loaded CACNP on MCF-7 (Hamidu 2019). MCF-7 cells were more sensitive to free doxorubicin compared with doxorubicin-loaded CACNP at 24 h and 48 h treatment duration, while at 72 h, cells were more sensitive to doxorubicin-loaded CACNP compared with free doxorubicin. The SEM findings were as described by Kamba et al. (2013a).

Gold–CACNP hybrid nanoparticle cytotoxicity studies on MCF7 revealed progressive decrease in percentage cell viability as the dose of increase from 0 to 100 $\mu\text{g}/\text{ml}$ (Kiranda et al. 2018). Free docetaxel and docetaxel-loaded CACNP revealed a progressive reduction in percentage viability of MCF-7 cancer cells in a dose- and time-dependent manner (Hammadi 2017a). MCF-7 was observed to be more sensitive to free docetaxel compared with docetaxel-loaded CACNP. At a maximum dose of 2 $\mu\text{g}/\text{ml}$, percentage viability of MCF-7 was 55% and 60% after exposure to free docetaxel and docetaxel-loaded CACNP, respectively, for 24 h; 22% and 27%, respectively, after 72-h treatment. Hammadi (2017a) stated that a lower amount of docetaxel released from the CACNP was responsible for the increased cell viability as compared with free docetaxel. Less than 80% of the drug bound to the CACNP was released to the cells within the treatment period.

In vitro efficacy of docetaxel-loaded CACNP on 4T1 mouse breast cancer cell line was carried out by Hammadi (2017b). MTT, Annexin V apoptotic assay, cell cycle analysis, scratch assay, scanning and transmission electron microscopy were carried out. The percentage cell viabilities at 24 h were above 50% at all concentrations of docetaxel and docetaxel-loaded CACNP. However, docetaxel-loaded CACNP group had a significant higher percentage cell viability compared with free docetaxel at

0.0625–0.5 µg/ml concentrations. At 48 and 72 h, there was no significant difference in percentage cell viability of docetaxel and docetaxel-loaded CACNP groups. There was no significant difference in Annexin V assay in both free docetaxel and docetaxel-loaded CACNP groups. Cell cycle arrest at subG0 and G2/M phases was noticed in both groups. SEM showed presence of cell membrane blebbing, while TEM showed nuclear fragmentation and vacuolation. Reduced cell migration was recorded in both free docetaxel and docetaxel-loaded CACNP groups with no significant difference. It was therefore concluded that docetaxel-loaded CACNP and free docetaxel has similar anticancer effects on 4T1 cells (Hammadi 2017b).

In vivo therapeutic study of docetaxel and docetaxel-loaded CACNP in Balb/C mice after inoculating with 4TI cells in the right mammary fat pad was carried out by Hammadi (Hammadi 2018). No mortality was recorded in docetaxel and docetaxel-loaded CACNP group. Tumour volume, organ weight, tumour inhibition rate, and tumour metastatic score were significantly lower in docetaxel-loaded CACNP 10 mg/kg group (Hammadi 2018).

Ibiyeye et al. (2019) evaluated the effect of doxorubicin and thymoquinone-loaded CACNP on MDA MB 231 breast cancer cell line. The free drugs were more effective in reducing the cell viability of MDA-MB-231 cells when compared with the drug-loaded CACNP except doxorubicin- thymoquinone-loaded CACNP which inhibited the growth of breast cancer cells than free doxorubicin/thymoquinone combination. Decrease in cell number was noted in all treatments as compared with control; this was most obvious in the doxorubicin–thymoquinone-loaded CACNP group. SEM revealed membrane blebbing, cell shrinkage and apoptotic bodies. Doxorubicin- thymoquinone-loaded CACNP treated group also showed cell membrane disruption. Annexin V apoptosis assay, doxorubicin-loaded CACNP was more effective in inducing apoptosis compared with free doxorubicin at 48 h. At 24 and 72 h there was no significant difference in the induction of apoptosis in free doxorubicin and doxorubicin-loaded CACNP. Doxorubicin–thymoquinone-loaded CACNP has the highest percentage of apoptotic and necrotic cells. Doxorubicin–thymoquinone-loaded CACNP has the most percentage of in SubG0. Most of the treatments cause significant S-phase arrest at 72 h. Free doxorubicin–thymoquinone was the most effective in inhibiting MDA-MB-231 cells metastasis. Nonetheless, doxorubicin–thymoquinone-loaded CACNP reduced cell metastasis more effectively than doxorubicin-loaded CACNP and thymoquinone-loaded CACNP. Ibiyeye et al. concluded doxorubicin-thymoquinone-loaded CACNP was the most efficient in eliminating breast cancer cells at lower dose of doxorubicin and thymoquinone (Ibiyeye et al. 2019).

Application of drug-loaded CACNP on breast cancer stem cells

Ibiyeye and Zuki (Ibiyeye and Zuki 2020) generated MDA MB231 3D cancer stem cells enriched mammosphere and the influence of combined doxorubicin–thymoquinone-loaded CACNP as well as single loaded drugs and free drugs was evaluated. Cancer stem cells were sensitive to doxorubicin-loaded CACNP and doxorubicin–thymoquinone-loaded CACNP and more resistance to free doxorubicin and doxorubicin–thymoquinone. Doxorubicin–thymoquinone-loaded CACNP also induced apoptosis in the CSCs compared to single drug-loaded CACNP. Free doxorubicin–thymoquinone

and doxorubicin–thymoquinone-loaded CACNP had the smallest size mammospheres compared with control after day 10 of treatment. Scanning electron microscope showed cell shrinkage, poor spheroid formation, distortion of the spheroid architecture. Doxorubicin–thymoquinone-loaded CACNP treated mammosphere had the worse abnormal surface morphology compared to the other treatment. All treatment showed non-specific cell cycle arrest (Ibiyeye and Zuki 2020).

The effect of drug-loaded CACNP on CSCs ALDH activity, surface marker expression, self-renewal capacity and metastatic potential was also assessed by Ibiyeye and Zuki (2020). Doxorubicin–thymoquinone-loaded CACNP was the most effective in preventing CSCs self-renewal, thereby, selectively targeting CSCs. Doxorubicin–thymoquinone-loaded CACNP suppressed the expression of CD44⁺ CD24^{low/–} cancer stem cell surface marker the most at both days 3 and 10, while ALDH activity was reduced to zero percent and the percentage of viable cells was also reduced to 0.1% at day 10. Ibiyeye and Zuki stated that high ALDH1 activity correlates with poor prognosis in breast cancer patients and has been associated with chemo/radio-resistance and poor prognosis, therefore, doxorubicin-thymoquinone-loaded CACNP can help reduce chemo/radio-resistance and improve prognosis in breast cancer patients. Doxorubicin-thymoquinone-loaded CACNP was most effective among the loaded CACNP in reducing CSCs migration and invasion. The study concluded that doxorubicin-thymoquinone-loaded CACNP may serve as a potential curative strategy for the management of breast cancer recurrence and metastasis (Ibiyeye and Zuki 2020).

Application of drug-loaded CACNP on bone cancer

Kamba et al. (2013b) studied the in vitro delivery and controlled release of doxorubicin-loaded CACNP in osteosarcoma bone cancer cells. MG 63 osteosarcoma bone cancer cells was treated with 0 to 2 µg/ml of free doxorubicin and doxorubicin-loaded CACNP for 24, 48 and 72 h. It was observed that the cell inhibition rate was dependent on concentration and incubation periods. MG 63 cells was more sensitive to free doxorubicin at 24 and 48 h. However, at 72 h it was observed that MG 63 cells was more sensitive to doxorubicin-loaded CACNP. Cell proliferation was evaluated with BrdU assay. Doxorubicin-loaded CACNP significantly suppressed MG 63 cells proliferation in a dose and time-dependent manner. Up-regulation of p53 gene, caspases 9, 8, 3, Bax and down-regulation of the Bcl-2 protein was observed in a concentration dependent manner. Kamba et al. postulated that the mechanisms by which doxorubicin-loaded CACNP cause cell death in MG 63 osteosarcoma bone cancer cells is by induction of apoptosis through up-regulation of p53, caspases 9, 8, 3 and Bax and down-regulation of Bcl-2 (Kamba et al. 2013b).

Fu (2017) evaluated the effects of doxorubicin-loaded CACNP on the UMR-106 cells. The concentrations 0.125 to 1 mg/ml of free doxorubicin were more sensitive to UMR-106 cells. Fu et al. stated that this may be because free doxorubicin is immediately contacted with the cells, which may induce toxicity to the cells unlike the doxorubicin encapsulated in CACNP. Though at 2 mg/ml concentration, doxorubicin-loaded CACNP showed similar cell viability as free doxorubicin. Fu et al. noted that, doxorubicin-loaded CACNP showed a similar reduction in cell viability as free doxorubicin in a concentration and time-dependent manner. Morphological observations by light microscopy

revealed decreased number of the cells, cell shrinkage, and detachment. Characteristic ultra-structural changes observed by SEM include microvilli disappearance, cell shrinkage, membrane blebbing and apoptotic bodies. TEM micrographs showed cell shrinkage, chromatin condensation. In addition, a large number of vesicles were noticed in the cytoplasm of cells treated with doxorubicin-loaded CACNP and few vacuoles containing doxorubicin-loaded CACNP coacervates. Doxorubicin and doxorubicin-loaded CACNP induced apoptosis in UMR-106 cells in a time-dependent manner. Doxorubicin-loaded CACNP induced cell cycle arrest, which was consistent with the mechanism of doxorubicin (Fu 2017).

Fu and colleagues (2018) induced osteosarcoma in orthotopic rat by injecting UMR-106 cells into the tibia cavity. Osteosarcoma induced was at least pathological stage-III and radiographs revealed expansible osteolytic lesions. Five groups including control, osteosarcoma model group, 2 mg/kg free doxorubicin group and two groups of doxorubicin-loaded CACNP (2 mg and 1.5 mg of corresponding doxorubicin/kg, respectively). There was no significant difference in the body weights gain in all treatment groups compared with control. However, there was significant difference in doxorubicin-loaded CACNP groups' body weight gain when compared to the free doxorubicin group. 50% of the rats in the free doxorubicin group died while only 16.7% mortality was recorded in 2 mg doxorubicin-loaded CACNP group. Zero percentage mortality was recorded in 1.5 mg doxorubicin-loaded CACNP group. Fu and colleague noted that doxorubicin-loaded CACNP is less toxic than the free doxorubicin. There was no significant difference in tumour growth suppression and reductions in the relative tumour volume in the doxorubicin-loaded CACNP groups and free doxorubicin group. However, there was significant difference when compared with osteosarcoma model group. X-ray radiographs showed reduction in osteolytic lesions and increased bone remodeling in doxorubicin-loaded CACNP groups and free doxorubicin group. Serum creatine kinase increased significantly in the free doxorubicin group as compared with control group, however, a significant reduction in serum creatine kinase were found in the doxorubicin-loaded CACNP groups when compared with free doxorubicin. Control and osteosarcoma model groups showed normal myocardium with no pathologies seen. Free doxorubicin caused obvious cardiac tissue vacuolar degeneration, hypertrophy and disruption of cardiac muscle fibres, and myocardia fibrous necrosis. However, mild changes were seen in the doxorubicin-loaded CACNP groups. Fu et al. explained that CACNP ensured little to no release of doxorubicin from CACNP into the circulation which resulted in the absence of doxorubicin-related cardiotoxicity seen in doxorubicin-loaded CACNP groups. There was no significant changes in serum aspartate aminotransferase, alanine aminotransferase and alkaline phosphatase. Histological examination revealed an obvious reduction in the average tumour cell numbers in free doxorubicin and the doxorubicin-loaded CACNP groups. Both doxorubicin-loaded CACNP groups and free doxorubicin group effectively inhibit tumour growth, reduce tumour mass and inhibit lung metastasis. The study concluded that the doxorubicin-loaded CACNP can significantly reduce osteosarcoma tumour volume and doxorubicin-related cardiotoxicity. 1.5 mg doxorubicin-loaded CACNP showed the comparable anticancer effect as 2 mg doxorubicin-loaded CACNP, suggesting that CANP will allow reduction in chemotherapy doses (Fu 2018).

Danmaigoro and colleagues (2019) explore the responses of doxorubicin-loaded CACNP on tumour bearing dogs, including osteosarcoma, in a single centred open clinical trial. No severe reactions to doxorubicin-loaded CACNP were observed. Partial response and progressive canine RECIST response were observed in the 15 weeks study period. Nonetheless, osteoid matrix production and osteogenic cell death and cell proliferation inhibition were recorded.

Applications of drug-loaded CACNP of leukemic cells

Ghaji (Ghaji 2018) studied CACNP as a cytarabine carrier against HL-60 human leukaemia cells and as anticancer therapy in leukaemia-bearing SCID mice. The IC₅₀ values of cytarabine and cytarabine-loaded CACNP were 5 µg/ml and 2.5 µg/ml, respectively at 72 h. 2.5 µg/ml cytarabine-loaded CACNP was more effective in inducing apoptosis than 5 µg/ml free cytarabine. SEM observations in both cytarabine and cytarabine-loaded CACNP revealed disappearance of microvilli, membrane blebbing, cell shrinkage and apoptotic bodies. Blood and bone marrow smear, and histological examination of major organs revealed that CACNP significantly enhances the effects of cytarabine in leukaemia-bearing SCID mice (Ghaji 2018).

Conclusions

Cockle shell-derived aragonite calcium carbonate nanoparticles (CACNP) have shown high loading capacity for both hydrophilic and hydrophobic drugs. It is safe in non-neoplastic cells and drug-loaded CACNP have shown significant antitumor effect in cancers including breast, osteosarcoma, leukaemia, and breast cancer stem cells. More research is however required in the antitumor effect in other cancers like brain, lung, liver, pancreatic and more. This review also recommends more research in functionalization of CACNP to actively target cancer stem cells by decorating it with hyaluronic acid, anti CD44 antibody or any other substrate specific to various cancer stem cells. Molecular studies on the drug-loaded CACNP needs to be elaborated.

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